

Physical plasticity of the nucleus in stem cell differentiation

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Cell differentiation in embryogenesis involves extensive changes in gene expression structural reorganization within the nucleus, including chromatin condensation and nucleoprotein immobilization. We hypothesized that nuclei in naive stem cells would therefore prove to be physically plastic and also more pliable than nuclei in differentiated cells. Micromanipulation methods indeed show that nuclei in human embryonic stem cells are highly deformable and stiffen 6-fold through terminal differentiation, and that nuclei in human adult stem cells possess an intermediate stiffness and deform irreversibly. Because the nucleo-skeletal component Lamin A/C is not expressed in either type of stem cell, we knocked down Lamin A/C in human epithelial cells and measured a deformability similar to that of adult hematopoietic stem cells. Rheologically, lamin-deficient states prove to be the most fluid-like, especially within the first ≈ 10 sec of deformation. Nuclear distortions that persist longer than this are irreversible, and fluorescence-imaged microdeformation with photobleaching confirms that chromatin indeed flows, distends, and reorganizes while the lamina stretches. The rheological character of the nucleus is thus set largely by nucleoplasm/chromatin, whereas the extent of deformation is modulated by the lamina.

chromatin remodeling | cell mechanics | nuclear plasticity

Developmental “plasticity” generally refers to a cell’s ability to modulate its gene expression (1) and often reflects changes in chromatin structure (2). Stem cell nuclei are therefore said to be more plastic than fully differentiated cells (3). Major differences are indeed found in chromatin conformation (4, 5), nuclear protein expression (6–8), and also DNA and histone modification (9). Differentiation further entails immobilization of some nucleoplasmic proteins and is said to functionally “rigidify” the genome, setting a relatively permanent preference for particular expression profiles (10, 11). Motivated by such remodeling, we sought to directly assess collective physical properties of the nucleus in differentiation.

In an embryo, more deformable nuclei could confer a significant advantage to less differentiated cells that must squeeze their way through developing tissues. Remarkably large nuclear deformations are seen, for example, during the migration of stem cell-like progenitor cells in brain tissue (Fig. 1A Upper) (12). Although such data illustrate deformability, we hypothesized that the nuclei of stem cells would prove more deformable, and it is indeed shown by micropipette aspiration that stem cell nuclei deform to a greater extent under a fixed stress compared with typical differentiated cell types. We go on to characterize the time-dependent deformation or creep under a constant applied stress and then also once the stress is removed from the nucleus. In the latter phase, we provide evidence of physical plasticity in which irreversible deformations persist without fracture. Single chromatin fibers in forced extension also exhibit plasticity, based perhaps on dissociation of histones from DNA (13–15). Our recent work on adult stem cells has additionally shown that multipotent cells are highly contractile and can generate significant cytoskeletal stress (16), representing a potential driving

force not only for cell motility (e.g., Fig. 1A) but also for nuclear remodeling. Here we assess some of the macromolecular determinants of nuclear deformability by fluorescence-imaged microdeformation (Fig. 1A), combined with quantitative stress measurements, photobleaching, and knockdown of lamin proteins at the periphery of the nucleus.

Results and Analysis

Nuclei in Stem Cells Deform More Readily than in Differentiated Cells.

To controllably assess the deformability of nuclei as stem cells differentiate, live cell microaspiration of nuclei within primary human embryonic stem cells (ESCs) was performed. Pluripotent cells (day-0) with fluorescently labeled nuclei were aspirated at constant pressure and compared with cells at days 2 and 6 after induction to neuroectodermal differentiation (17). The ratio of nuclear projection length to cell membrane extension ($L_{\text{nuc}}/L_{\text{cell}}$) after 1 min of fixed pressure aspiration provides a first simple metric of relative nuclear deformability (Fig. 1B); this ratio is near unity for highly deformable nuclei, and it is low for very stiff nuclei. We find that ESC nuclei are highly deformable and that they stiffen over several days in culture, approaching a 6-fold higher relative stiffness of 0.15 that is typical of differentiated cells such as embryonic fibroblasts (Fig. 1C). An empirically fit exponential yields an effective time constant of 2.7 days for differentiation-associated stiffening of the nucleus relative to the cell body; this timescale appears roughly consistent with global changes in nucleoprotein expression such as lamins in ESCs (7, 17). The limiting ratio for $L_{\text{nuc}}/L_{\text{cell}}$ (i.e., nuclear:cytoplasmic stiffness) of ≈ 0.15 is also consistent with past measurements of relative nuclear compliance for other differentiated cells (18).

Hematopoietic stem cells (HSCs) obtained from bone marrow are less multipotent than ESCs, but HSCs can still differentiate into all of the mature blood cell types (19) as well as a few solid tissue cells that include epithelial cells (20). Micropipette aspiration of human-HSC nuclei subjected to a step increase in pressure show progressive flow into the pipette, and these stem cell nuclei again exhibit greater deformation than fibroblast nuclei at the same stress (Fig. 2B and C): HSC nuclei deform more than twice as much after 200 sec of aspiration. A relative deformability for HSC nuclei of $L_{\text{nuc}}/L_{\text{cell}} \approx 0.5$ identifies HSCs as roughly equivalent to ESCs at day 3 ± 1 (Fig. 1C). On the basis of this physical measure, HSCs would be rightly viewed as partially differentiated.

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Abbreviations: ESC, embryonic stem cell; HSC, hematopoietic stem cell; shRNA, small hairpin RNA.

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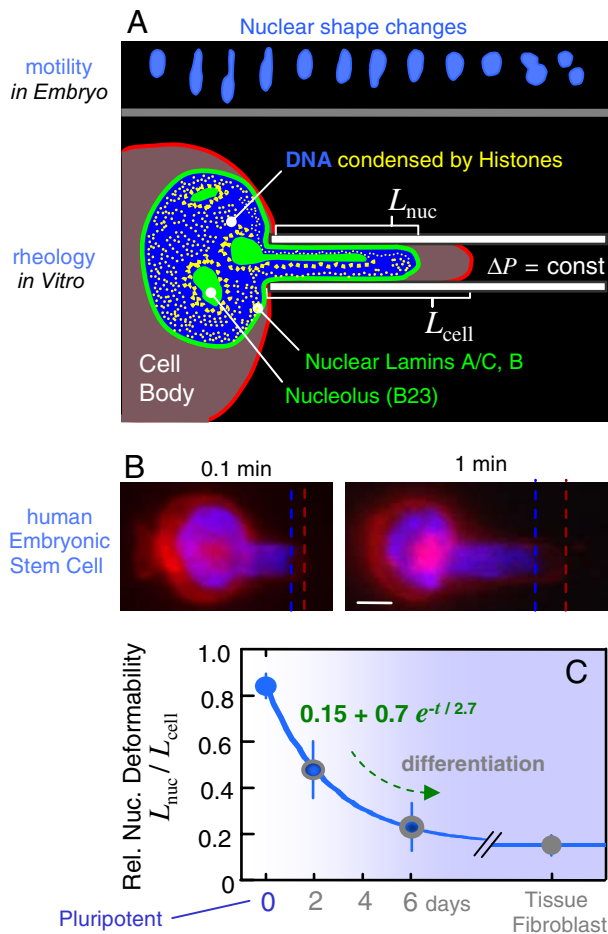


Fig. 1. Nuclei of human stem cells are more deformable than nuclei of differentiated cells. (A Upper) Neural progenitor cell nuclei (12) show large deformations during *in vivo* migration (SI Fig. 8). Micropipette aspiration mimics such distortions. (B) Human ESCs were aspirated after differentiation in culture, and the ratio of nuclear extension to cytoplasmic extension was measured as $L_{\text{nuc}}/L_{\text{cell}}$. A day-0 pluripotent ESC is shown with fluorescent dyes labeling nuclear DNA (blue) and the cell membrane (red). (Scale bar: $3 \mu\text{m}$.) Dead cells were excluded by counterstaining with propidium iodide. (C) As differentiation progresses, ESC nuclei stiffen nearly 6-fold relative to cytoplasm, and the decrease in relative compliance fits an exponential decay. Differentiated cells such as embryonic fibroblasts also have a nucleus that is stiffer than the cytoplasm. Aspiration of at least three cells and two to three time points per cell were analyzed for each “day” (average \pm SD).

Nuclei Exhibit Power Law Creeping Flow. Aspiration of the various nuclei with a step in pressure shows an increase in $L_{\text{nuc}} = L(t)$ over long times (200 sec) and also, upon release of the applied stress, a permanent deformation (Fig. 2A). The response in the recovery phase provides clear evidence of plasticity during the aspiration phase, but first we characterize the flow behavior, or rheology (21), of the aspiration phase. $L(t)$ is scaled by pipette diameter D and aspiration pressure ΔP to obtain a creep compliance.

$$J(t; \Delta P) = \frac{4\pi}{3} \Phi \frac{L}{D} \frac{1}{\Delta P} \quad [1]$$

The constant $\Phi = 2.1$ (22). On a log-log scale, the data for HSC and fibroblast nuclei exhibits regime(s) of power law behavior that fit the following form.

$$J(t; \Delta P) = A \cdot (t/t_0)^\alpha \quad [2]$$

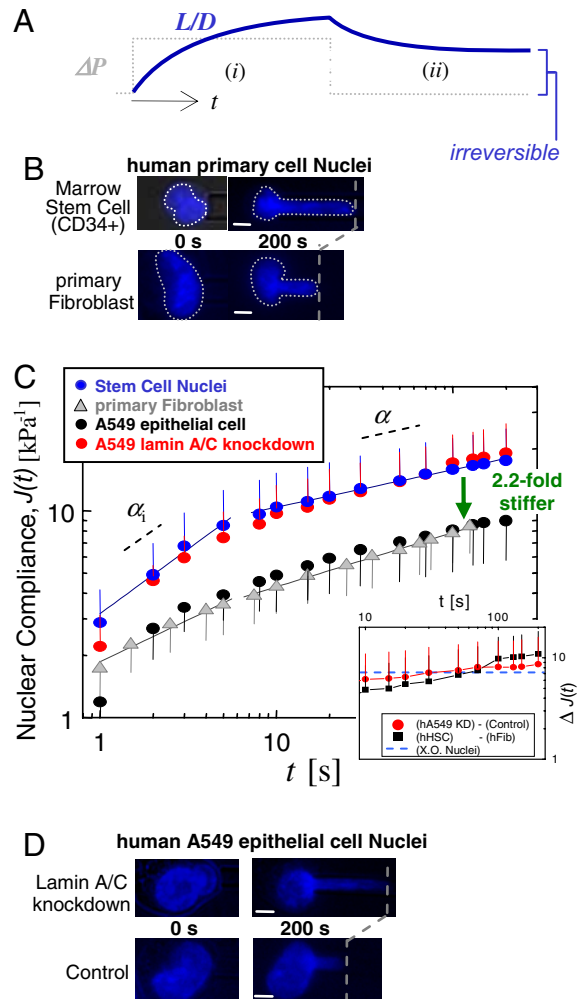


Fig. 2. Marrow-derived human HSCs have more compliant nuclei than primary human fibroblasts, which may correspond to a lack of Lamin A/C. (A) Constant pressure aspiration into a micropipette (diameter, D) with creep compliance response for relative aspirated length L/D (*i*). Release of ΔP and incomplete recovery of L/D (*ii*). (B–D) After 200 sec of aspiration, HSC nuclei (blue) have deformed 2.2-fold more than fibroblast nuclei (gray), indicating that the latter are stiffer. A549 cells (black) are made equally compliant by knockdown of Lamin A/C (red) (average \pm SD; $n = 15$ –20 nuclei). (Scale bars: $3 \mu\text{m}$.)

The prefactor A has units of inverse pressure or stiffness [kPa^{-1}] and, to facilitate comparisons to past experiments on nuclei conducted on approximately second timescales (22, 23), $t_0 \equiv 1$ sec. This t_0 conforms to the convention for rheological coefficients (having units: Pa sec^α) and is also the earliest measurable timescale in our experiments. Eq. 2 captures a wide range of mechanical responses, from simple to complex: $\alpha = 0$ indicates a simple elastic solid and $\alpha = 1$ indicates a simple fluid. An intermediate power law is indicative of a viscoelastic or viscoplastic response. Cytoskeletal rheology often yields $\alpha \approx 0.2$ – 0.3 (24, 25), which is understood to reflect a broad spectrum of characteristic timescales and is typical of complex macromolecular structures. Additionally, while fractal organization of chromatin density within the nucleus (26) provides a possible structural basis for a wide range of characteristic times, theory for simple polymer gels gives $\alpha = d_f/(d_f + 2)$, with d_f the fractal dimension of the gel (27). Such a relation suggests that a higher α corresponds to a higher d_f , which is consistent with a significantly higher d_f of decondensed chromatin after treatment with a histone deacetylase inhibitor (26).

We find that fits of Eq. 2 to the HSC results as well as to the Lamin A/C-knockdown results split into two phases below and above ≈ 10 sec [Fig. 2C and supporting information (SI) Fig. 9]. For consistency we also separate the remaining aspiration data into two regimes (see Fig. 5A and SI Tables 1 and 2). In the initial phase, HSC results fit with $\alpha_i \approx 0.60$, indicating greater fluidity than fibroblasts with $\alpha_i \approx 0.41$ (SI Table 1). Beyond 10 sec, the creep slows for both types of nuclei, and $\alpha \approx 0.2$ indicates a more solid-like behavior. Relating these power law exponents to specific fractal dimensions is beyond the scope here and is a general challenge even in simple systems (27).

Network of Lamin A/C Modulates Nuclear Compliance. Differentiation of ESCs entails changes in multiple structural components of the nucleus, including altered expression of Lamin proteins (A/C and B) (7), as well as changes in the extent of heterochromatinization (10). Neither ESCs nor HSCs have detectable levels of Lamin A/C (28) (confirmed by immunofluorescence and blotting), and so we hypothesized that observed changes in nuclear rheology reflect altered Lamin A/C expression. To mimic this aspect of the stem cells with the human-derived epithelial cell line A549, we knocked down Lamin A/C by $>85\%$ with plasmid-based small hairpin RNA (shRNA) mediated interference (SI Fig. 10A). While immunofluorescence detected little to no change in either Lamin B expression or key chromatin modification markers of the cell's differentiated state (SI Fig. 10B), the A549 Lamin A/C knockdowns exhibit a nuclear rheology that is indistinguishable from that of HSCs (Fig. 2C), whereas the rheological properties of untreated A549 cells prove very similar to those of committed fibroblasts (Fig. 2C, black and gray symbols). Changes in Lamin A/C are therefore sufficient to cause a ≈ 2 -fold difference in stiffness (Fig. 2 B–D). Also, although the extent of deformation is dramatically altered by changes in Lamin A/C expression, the characteristic power law in creeping flow of nuclei is unaffected by Lamin A/C knock-down. Underlying rheological properties of nuclei might therefore be lamin-independent.

Our recent compliance measurements of the *Xenopus* oocyte (XO) nucleus provide a useful comparison because the mechanics of XO nuclei are dominated by the lamin network that surrounds dilute chromatin (29). We find here that J_{XO} approximates the difference in nuclear compliance (ΔJ) between HSCs and fibroblasts as well as between A549 controls and A549-Lamin-knockdowns (Fig. 2C Inset). A stiff lamina thus seems likely to explain nuclear stiffening in late differentiation.

Chromatin Is Stiff When Condensed but Otherwise Flows. The remarkable compliance of nuclei in pluripotent ESCs (Fig. 1A) seems likely to reflect high accessibility of chromatin (10). Some terminally differentiated nuclei have, in contrast, highly condensed chromatin that might be expected to be stiff (30). Divalent cations such as Ca^{2+} and Mg^{2+} will condense nuclei (22, 31), and so we introduced these ions into nuclei via selective permeabilization of the cell membrane by the detergent digitonin, which does not permeabilize the nuclear membrane. Condensation by divalent cations results in extremely stiff nuclei with small values for the creep compliance factors A and α (Fig. 3). Similar effects were seen with the ionophore A23187, which more selectively permeabilizes the plasma membrane to Ca^{2+} .

The lamin-independent nature of nuclear flow (i.e., $\alpha \approx 0.2$), combined with the strong effects of condensation, implicates chromatin in the physical plasticity of the nucleus. We therefore tracked chromatin with GFP-histones (H2B), as well as GFP Lamin A in TC7 epithelial cells. A dark stripe of GFP-H2B was made by laser photobleaching (FRAP/FIMD, fluorescence recovery after photobleaching/fluorescence-imaged microdeformation). The parabolic flow profile of fluorescence proves consistent with a strong but sheared linkage between chromatin

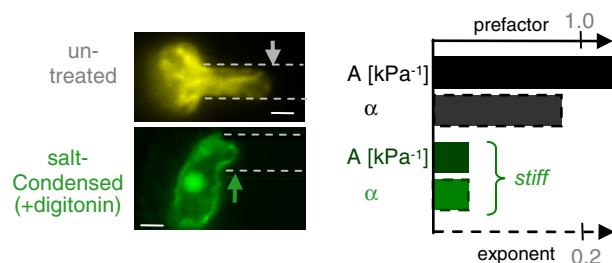


Fig. 3. Divalent salts condense chromatin and stiffen the nucleus. Compared with untreated nuclei, quantification reveals decreases in both the creep prefactor, A , and the creep exponent, α , due to cation-induced condensation. (Scale bar: $3 \mu\text{m}$.)

and the lamina (Fig. 4A and SI Fig. 11). Axial intensity profiles show that chromatin is progressively compacted toward the tip as the bleached stripe convects during aspiration. In some nuclei, chromatin bundles align and visibly extend within the pipette, indicative of physical remodeling (SI Fig. 11, asterisk).

GFP-Lamin A stretches during aspiration (Fig. 4B), with widening of the bleached stripe and lengthening of the unbleached tip area, which also thins as it stretches. The lack of recovery of the photobleached region provides direct evidence that large, sustained strains do not significantly increase Lamin A incorporation into the nuclear lamin over the experimental timescale. In unbleached nuclei, the observed gradient in density is similar to that of other elastic networks, particularly the red cell spectrin network (32) and the nuclear lamina of both HeLa cells and mouse embryonic fibroblasts (23).

Labeling nucleoli with GFP-B23 (nucleophosmin) reveals slow nucleolar extrusion into the pipette during aspiration (Fig. 4C), as quantitated by the decreased distance from nucleolus-to-tip ($L - L_{\text{neol}}$). Further kinematic analyses (SI Figs. 12 and 13) suggest nucleoli are stiffer than nucleoplasm, consistent perhaps with higher electron density in EM imaging as well as reduced

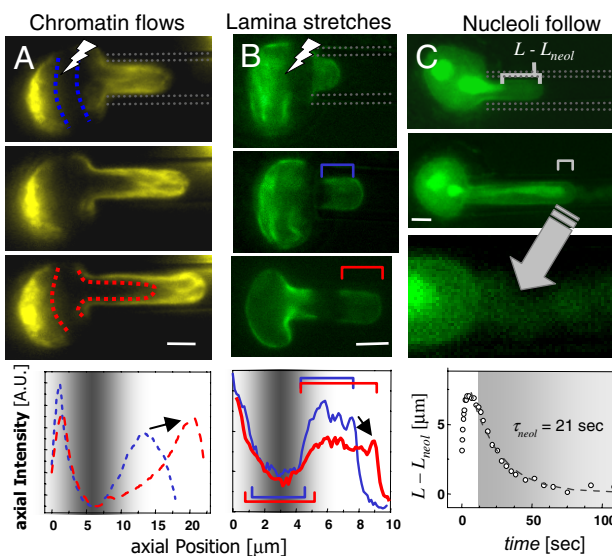


Fig. 4. Distinctive mechanics of nuclear components. (A) FRAP of GFP-H2B chromatin (pseudocolored yellow) reveals chromatin flow within the pipette. Chromatin compaction at the tip is quantified in the axial intensity profiles, and the arrow indicates an increase in intensity with compaction. (B) The lamina (green) is stably stretched into the pipette, and the arrow indicates a decrease in intensity with dilation. (C) Nucleoli slowly follow chromatin toward the nuclear tip, as GFP permeates the intact envelope (arrow into magnified view in bottom panel). (Scale bar: $3 \mu\text{m}$.)

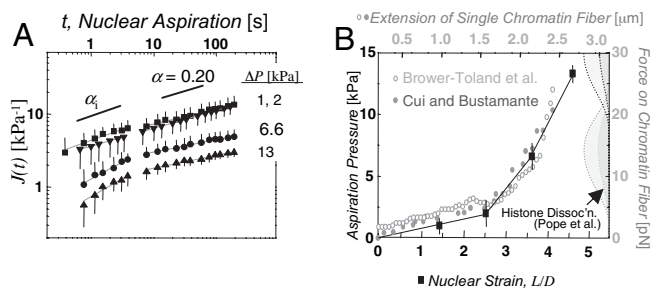


Fig. 5. Scale-free creep of nuclei, and nonlinear stress-strain mapping onto chromatin fiber data. (A) Nuclear creep in TC7 cells as a function of pressure (average \pm SD; $n = 10$ –15 nuclei). At large ΔP , J shows a crossover at $\tau_{\text{plastic}} \cong 8$ –10 sec. (B) Overlay of nuclear aspiration results and single chromatin fiber extension data (13, 14). The data from Brower-Toland *et al.* is normalized to the initial length of the Cui and Bustamante fiber, and stretched by a factor of 1.75. The histograms on the right indicate force-dependent frequency of histone dissociation (15).

accessibility of intranuclear dextran (33). Visible loss of soluble GFP from the nucleus (Fig. 4C, arrow) indicates slow flow through the nucleus into the pipette, but the intact appearance of the lamina suggests permeation through nuclear pores, consistent with nuclear export processes (34).

Plastic Flow of Nuclei and Nucleoli Maps into Chromatin Fiber Compliance. Distortions seen in chromatin and nucleoli are large and occur on both short timescales, as viscoelastic deformation, and on long timescales under small stress, consistent with plastic flow (21). To quantify these regimes and to also relate chromatin deformation within the nucleus to nonlinear extension forces known for isolated chromatin (13–16), four different aspiration stresses were applied to individual nuclei (Fig. 5A). At low ΔP of 1–2 kPa, the creep of differentiated cell nuclei is fit relatively well by a single power law. However, at larger stresses (≥ 6.6 kPa), a crossover time in the creep compliance is seen at $\tau_{\text{plastic}} \cong 8$ –10 sec. This is denoted as plastic because the small deformations ($L/D \sim 1$) held for short times $\leq \tau_{\text{plastic}}$ lead to essentially full recovery, contrasting with results below for long-time aspiration. For $t > \tau_{\text{plastic}}$, the nuclear creep exponent α proves independent of applied stress with $\alpha \cong 0.2 \pm 0.04$ (see SI Table 2), which is in agreement with results above as well as data on fully isolated nuclei in buffers low in divalent cations (21). At short times, $t \leq \tau_{\text{plastic}}$, the creep exponent α_i is distinctly higher and tends to increase with increasing stress, indicative of a more fluid-like character in

this initial regime. Stem cells also display biphasic behavior around $\tau_{\text{plastic}} \cong 10$ sec (Fig. 1C). We thus observe a stress-sensitive “fluidization” of all nuclei that is characterized by an increase in the initial creep exponent (α_i) with increasing stress. Stem cell nuclei, which are overall more compliant, are fluidized at lower stress (2 kPa) than the stiffer differentiated nuclei (6.6 kPa).

Nuclear compliance measurements and visualization of H2B reorganizations indicate a central role for chromatin mechanics, but additional analyses make a stronger case. $J(t, \Delta P)$ decreases strongly with pressure, indicating that the nucleus stiffens with increasing stress similar to experiments on single chromatin fibers. We plot the large strain L/D at 200 sec versus the applied stress (Fig. 5B), spanning the same experimental timescale for extensional studies of individual chromatin fibers: hundreds of nanometers per second for several micrometers over 15–30 sec (13, 14). Overlaying the force-extension behavior of chromatin fibers on the nucleus experiments presented here, we determined an effective chromatin fiber diameter d_{chrom} from the nuclear aspiration pressure ΔP and the force f per chromatin fiber, i.e., $d_{\text{chrom}} \sim (f \Delta P^{-1})^{1/2}$. The best fit yields $d_{\text{chrom}} \cong 45$ nm. This estimation should not be overinterpreted because it makes many naive assumptions, such as homogeneous stress in chromatin and aligned fibers, but the result is surprisingly close to the most recent measurements of bimodal chromatin fiber diameters of 33 nm and 44 nm (35). We speculate that the nonlinear nature of nuclear rheology might therefore be attributable to chromatin.

Irreversible Nuclear Deformation. Flow and irreversibility at the molecular scale often correspond to disruption and/or entanglement of macromolecular structures. Some of the past studies of isolated chromatin postulate the dissociation of nucleosomes in forced extension (13–15). To quantify changes in histone mobility in stressed nuclei, FRAP was applied to GFP-H2B on the highly extended chromatin within the pipette. Stressed or not, the mobile fraction of H2B remained low at $\approx 8\%$ (SI Fig. 11 C and D), which agrees with results from other cell lines (36). Fluorescent bundles of GFP-H2B also appear well defined without loss of resolution or intensity inside the pipette where stresses are clearly high (Fig. 4A and SI Fig. 11). The creeping flow in aspiration is therefore supported in part by changes in chromatin conformation.

In a final set of experiments focused again on plasticity, nuclei aspirated at the low stress of 2 kPa for 200 sec were allowed to recover after aspiration (Figs. 2A and 6). Even at this pressure, large and irreversible deformation is evident, with recovery of no more than 20% of the maximum L/D . The timescale of recovery

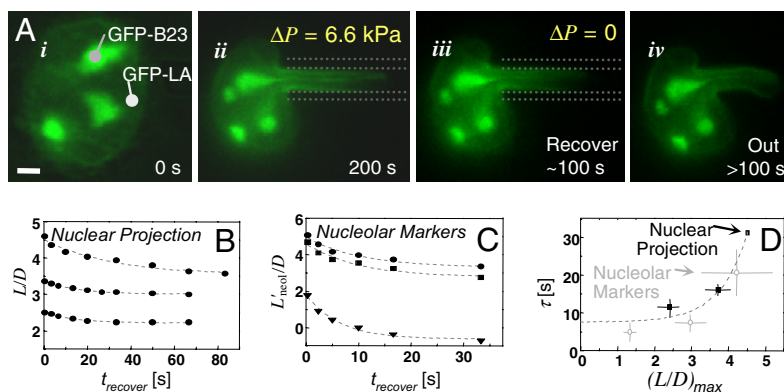


Fig. 6. *In situ* irreversibility of stretched nuclei. (A) The undeformed nucleus (i) is aspirated for ≈ 200 sec (ii). Recovery within the micropipette for ≈ 100 sec (iii) is followed by ejection from the pipette (iv). (Scale bar: 3 μm .) Plasticity is evident in the persistently deformed shapes of nuclei and nucleoli, and the time required for even partial recovery increases for both (B and C) at large deformations. (D) Extrapolation of the data to the small strain limit yields $\tau_{\text{recover}} \cong 8$ sec.

aspirating buffer (135 mM NaCl/5 mM KCl/5 mM Hepes/1.8 mM CaCl₂/2 mM MgCl₂/10% BSA, and the viability dye propidium iodide). At least 30 min before aspiration, differentiated cells were treated with 10 μM latrunculin A to depolymerize the actin cytoskeleton. Cells were loaded into a sample chamber that allows micropipette access from the side. Only nonphase, lucid viable cells that excluded propidium iodide were aspirated. Nuclei were visualized via Hoechst 33342 DNA dye (Invitrogen), and ESC plasma membranes were visualized by a fluorescently conjugated wheat germ

agglutinin. All chemicals were purchased from Sigma–Aldrich unless indicated. Further details of labeling and imaging are provided in *SI Methods*.

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- Blau H, Pavlath G, Hardeman E, Chiu C, Silberstein L, Webster S, Miller S, Webster C (1985) *Science* 230:758–766.
- Slack JMW, Tosh D (2001) *Curr Opin Genet Dev* 11:581–586.
- Szutorisz H, Dillon N (2005) *BioEssays* 27:1286–1293.
- Labrador M, Corces VG (2002) *Cell* 111:151–154.
- West AG, Fraser P (2005) *Hum Mol Genet* 14:R101–R111.
- Worman HJ, Courvalin, J-C (2005) *Int Rev Cytol* 246:231–279.
- Constantinescu D, Gray HL, Sammak PJ, Schatten GP, Csoka AB (2006) *Stem Cells* 24:177–185.
- McKittrick E, Gafken PR, Ahmad K, Henikoff S (2004) *Proc Natl Acad Sci USA* 101:1525–1530.
- Li E (2002) *Nat Rev Genet* 3:662–673.
- Meshorer E, Yellajoshula D, George E, Scambler PJ, Brown DT, Misteli T (2006) *Dev Cell* 10:105–116.
- Kosak ST, Groudine M (2004) *Science* 306:644–647.
- Tsai J-W, Chen Y, Kriegstein AR, Vallee RB (2005) *J Cell Biol* 170:935–945.
- Cui Y, Bustamante C (2000) *Proc Natl Acad Sci USA* 97:127–132.
- Brower-Toland BD, Smith CL, Yeh RC, Lis JT, Peterson CL, Wang MD (2002) *Proc Natl Acad Sci USA* 99:1960–1965.
- Pope LH, Bennink ML, van Leijenhorst-Groener KA, Nikova D, Greve J, Marko JF (2005) *Biophys J* 88:3572–3583.
- Engler AJ, Sen S, Sweeney HL, Discher DE (2006) *Cell* 126:677–689.
- Ozolek JA, Jane EP, Krowsoski LA, Sammak PJ (2007) *Stem Cells Dev* 16(3):403–412.
- Maniotis AJ, Chen CS, Ingber DE (1997) *Proc Natl Acad Sci USA* 94:849–854.
- Kondo M, Wagers AJ, Manz MG, Prohaska SS, Scherer DC, Beilhack GF, Shizuru JA, Weissman IL (2003) *Annu Rev Immunol* 21:759–806.
- Krause DS, Theise ND, Collector MI, Henegariu O, Hwang S, Gardner R, Neutzel S, Sharkis SJ (2001) *Cell* 105:369–377.
- Larson RG (1999) *The Structure and Rheology of Complex Fluids* (Oxford Univ Press, New York).
- Dahl KN, Engler AJ, Pajeroski JD, Discher DE (2005) *Biophys J* 89:2855–2864.
- Rowat AC, Foster LJ, Neilsen MM, Weiss M, Ipsen JH (2004) *J R Soc Interface* 2:63–69.
- Fabry B, Maksym GN, Butler JP, Glogauer M, Navajas D, Fredberg JJ (2001) *Phys Rev Lett* 87:148102.
- Hoffman BD, Massiera G, Van Citters KM, Crocker JC (2006) *Proc Natl Acad Sci USA* 103:10259–10264.
- Toth KF, Knoch TA, Wachsmuth M, Frank-Stohr M, Stohr M, Bacher CP, Muller G, Rippe K (2004) *J Cell Sci* 117:4277–4287.
- Scanlan JC, Winter HH (1991) *Macromol* 24:47–54.
- Olins AL, Herrmann H, Lichter P, Kratzmeier M, Doenecke D, Olins DE (2001) *Exp Cell Res* 268:115–127.
- Dahl KN, Kahn SM, Wilson KL, Discher DE (2004) *J Cell Sci* 117:4779–4786.
- Krauss SW, Lo AJ, Short SA, Koury MJ, Mohandas N, Chasis JA (2005) *Blood* 106:2200–2205.
- Engelhardt M (2004) *Biochem Biophys Res Commun* 324:1210–1214.
- Discher DE, Mohandas N, Evans EA (1994) *Science* 266:1032–1035.
- Gorisch SM, Lichter P, Rippe K (2005) *Histochem Cell Biol* 123:217–228.
- Yu Y, Maggi LB, Jr, Brady SN, Apicelli AJ, Dai MS, Lu H, Weber JD (2006) *Mol Cell Biol* 26:3798–3809.
- Robinson PJJ, Fairall L, Huynh VAT, Rhodes D (2006) *Proc Natl Acad Sci USA* 103:6506–6511.
- Kimura H, Cook PR (2001) *J Cell Biol* 153:1341–1354.
- Yellajoshula D, Brown DT (2006) *Proc Natl Acad Sci USA* 103:18568–18573.
- Yabuki M, Miyake T, Doi Y, Fujiwara T, Hamazaki K, Yoshioka T, Horton AA, Utsumi K (1999) *Physiol Chem Phys Med NMR* 31:77–84.
- Shav-Tal Y, Lee B-C, Bar-Haim S, Hadas S, Zipori D (2001) *J Cell Biochem* 81:379–392.
- Tamada H, Thuan NV, Reed P, Nelson D, Katoku-Kikyo N, Wudel J, Wakayama T, Kikyo N (2006) *Mol Cell Biol* 26:1259–1271.
- Broers JLV, Peeters EAG, Kuijpers HJH, Endert J, Bouten CVC, Oomens CWJ, Baaijens FPT, Ramaekers FCS (2004) *Hum Mol Genet* 13:2567–2580.
- Lammerding J, Schulze PC, Takahashi T, Kozlov S, Sullivan T, Kamm RD, Stewart CL, Lee RT (2004) *J Clin Invest* 113:370–378.
- Fong LG, Ng JK, Lammerding J, Vickers TA, Meta M, Cote N, Gavino B, Qiao X, Chang SY, Young SR, et al. (2006) *J Clin Invest* 116:743–752.
- Boguslavsky RL, Stewart CL, Worman HJ (2006) *Hum Mol Genet* 15:653–663.
- Favreau C, Higuete D, Courvalin J-C, Buendia B (2004) *Mol Cell Biol* 24:1481–1492.
- Brown JM, Leach J, Reittie JE, Atzberger A, Lee-Prudhoe J, Wood WG, Higgs DR, Iborra FJ, Buckle VJ (2006) *J Cell Biol* 172:177–187.
- Walter J, Schermelleh L, Cremer M, Tashiro S, Cremer T (2003) *J Cell Biol* 160:685–697.
- Manders EMM, Kimura H, Cook PR (1999) *J Cell Biol* 144:813–822.
- Cremer T, Cremer C (2001) *Nat Rev Genet* 2:292–301.
- Lammerding J, Hsiao J, Schulze PC, Kozlov S, Stewart CL, Lee RT (2005) *J Cell Biol* 170:781–791.
- Gorisch SM, Wachsmuth M, Ittrich C, Bacher CP, Rippe K, Lichter P (2004) *Proc Natl Acad Sci USA* 101:13221–13226.
- Tseng Y, Lee JSH, Kole TP, Jiang I, Wirtz D (2004) *J Cell Sci* 117:2159–2167.